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The pain and skeletal deformity associated with osteoporosis may secondarily reduce muscle strength, and this has been established through previous studies to be closely correlated with back extensor strength. In this study, we compared BES estimated using Electromyography (EMG) and inertial measurement units (IMU) sensors with BES measured by the hand-held dynamometer (HHD) and developed a more convenient method for measuring BES and confirmed its validity. Initially developed through clinical trials on healthy women, our lumbar paraspinal strength estimation formula was subsequently refined through empirical testing on osteoporosis patients.

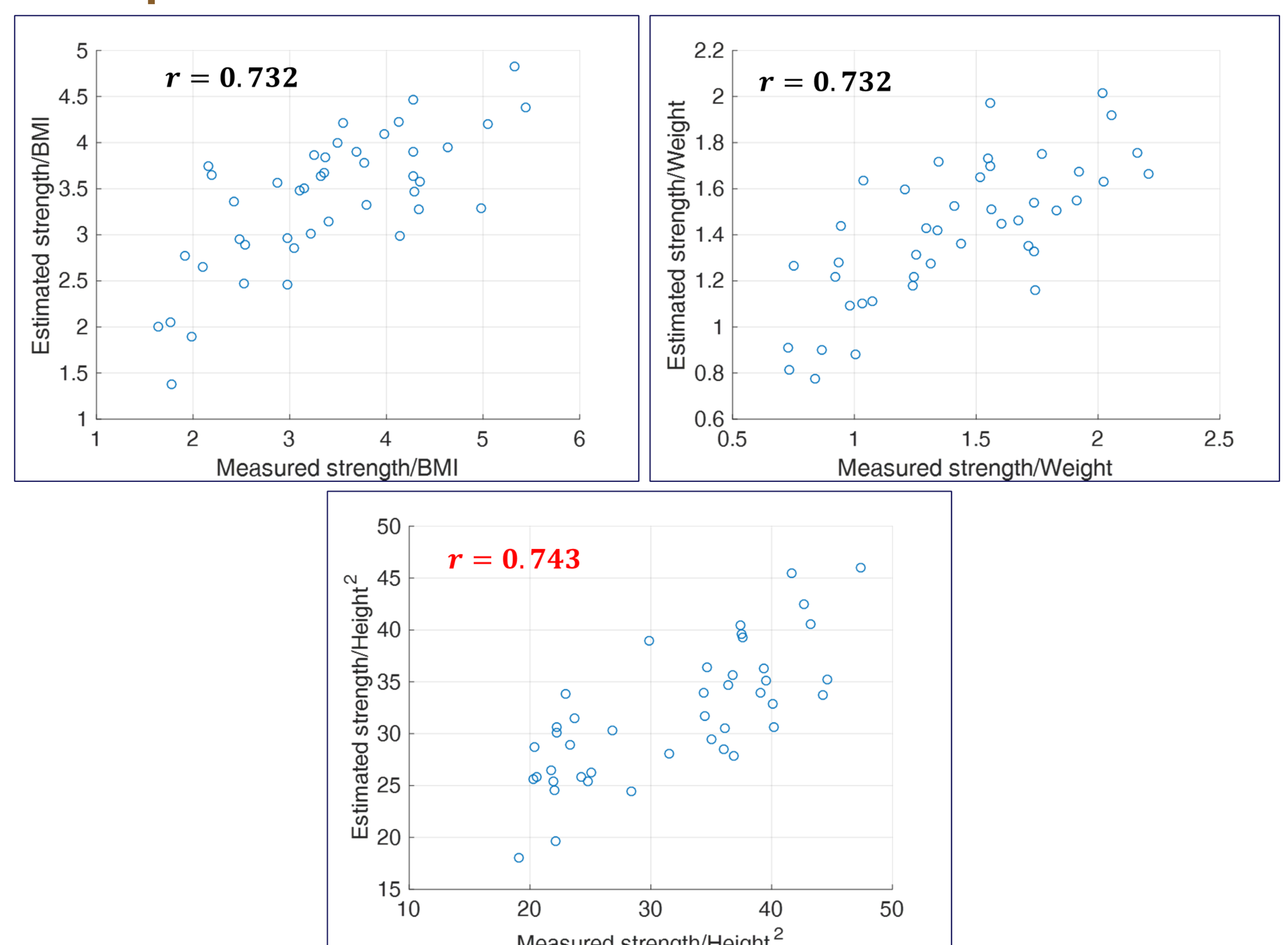
This study centers on postmenopausal women afflicted with osteoporosis (N=48) (table 1). Back extensor strength (BES) was assessed using Handheld Dynamometry (HHD) affixed with a Tripod & Belt system device in the prone position, with subjects exerting maximal effort to lift the upper body. Additionally, BES evaluations using EMG and IMU sensors were conducted during a single set of back extension exercises. EMG sensors were positioned at the L1 level, while IMU sensors were affixed to the interscapular area. Exercises comprised lifting the upper body from prone, sustaining for 5 seconds, resting for 10 seconds, repeated for 10 repetitions.

Baseline characteristics were depicted in Table 1. An estimation equation for BES was derived via multiple linear regression analysis. A novel system was devised to predict BES, as measured by HHD, utilizing EMG and IMU signals acquired during back extension exercises (Figure 1). Quantitative parameters were extracted from EMG and IMU data. Notably, these parameters demonstrated disparities compared to those osteoporosis of healthy controls in a prior study. Three distinct models were constructed, incorporating muscle strength relative to BMI, weight, and height² (figure 2). It was ascertained that the estimated BES index effectively approximated HHD-measured BES. Among the three indices, muscle strength/height² exhibited the strongest correlation with measured values ($r=0.743$, $p<0.001$).

The figure consists of three parts. At the top left is a diagram of a human torso from the back, showing the spine and shoulder blades. To its right is a graph titled 'Gyro X' showing angular velocity in degrees per second (gyro[deg/sec]) on the y-axis (ranging from -40 to 40) against time in seconds (time[s]) on the x-axis (ranging from 96 to 106). The graph shows a sharp positive peak around 98.5s, a period of near-zero activity labeled 'Hold the lift for 5 seconds' between 100s and 102s, and a sharp negative peak around 103.5s. Annotations with arrows point to these features: 'positive angular velocity when the upper body is raised' points to the first peak, and 'Negative angular velocity when the upper body goes down' points to the second peak. Below the diagram and the Gyro X graph is an EMG graph showing muscle activity in microvolts (amplitude [μ V]) on the y-axis (ranging from -600 to 600) against time in seconds (time[s]) on the x-axis (ranging from 0 to 180). The EMG signal shows periodic bursts of activity corresponding to the movements.

	Participants
Age (y)	69.13 ± 7.68
Height (cm)	154.61 ± 5.64
Weight (kg)	54.86 ± 7.24
BMI (kg/m²)	22.98 ± 3.03
HHD_max (N)	83.42 ± 34.73
HHD_mean (N)	75.91 ± 21.64
Right HGS (kg)	22.69 ± 4.58
Left HGS (kg)	21.32 ± 4.34
FTSST (s)	8.87 ± 2.13
30s SST	18.85 ± 5.07
SMI	6.72 ± 0.78

Fig 2. Development of BES estimation formula through multiple linear regression analysis in osteoporosis



A new method has been developed to measure the strength of the back extensor muscles, and it has been confirmed to be applicable to postmenopausal women with osteoporosis. Since a method for measuring back extensor strength in healthy young adults has already been developed in previous study, further research is needed to determine whether the back extensor measurement method can be used in screening for normal, osteopenic, and osteoporotic conditions.

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